



# Non-negative least-squares random field theory★



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We model imaging data at a voxel by a linear model with some or all coefficients constrained to be non-negative. The model is fitted by non-negative least-squares (NNLS) separately at every voxel. We wish to detect those voxels where the constrained coefficients are significantly positive. We present new random field theory results for finding the corrected P-value that allows us to detect such points. We apply these results to detecting activation in fMRI using a set of extreme HRF basis functions.

## Methods

The linear model for image data at a single voxel is

$$\mathbf{Y} = \mathbf{X}\beta + \mathbf{Z}\gamma + \epsilon, \quad \epsilon \sim N(0, \mathbf{C}\sigma^2)$$

where  $\mathbf{Y}$  is an observation vector,  $\mathbf{X}$  and  $\mathbf{Z}$  are design matrices common to every voxel,  $\beta$  and  $\gamma$  are vectors of unknown coefficients, and  $\epsilon$  is an error vector with unknown variance  $\sigma^2$  but a known correlation structure  $\mathbf{C}$  common to every voxel. Without loss of generality, we can assume that  $\mathbf{C}=\mathbf{I}$ , the identity matrix, by pre-whitening the model.

The important point is that  $\beta \geq 0$  (component-wise) whereas  $\gamma$  is arbitrary. Fitting the model by NNLS is straightforward [1]:

1. Do all subsets regression on  $\mathbf{X}$ .
2. Amongst the submodels with  $\beta > 0$ , select the submodel with the least error sum of squares,  $SSE_1$ .

Let  $SSE_0$  be the error sum of squares of the null model  $H_0 : \beta = 0$  and let  $\nu$  be its df. The NNLS test statistic of  $H_0$  is

$$F_{\text{NNLS}} = \frac{SSE_0 - SSE_1}{SSE_1/(\nu - 1)}.$$

The random field theory P-value of the  $F_{\text{NNLS}}$  SPM is [2]:

$$\mathbb{P}(\max F_{\text{NNLS}} \geq t) = \sum_{j=1}^{\nu-1} p_j \mathbb{P}\left(\max F_{j, \nu-j} \geq t \frac{\nu-j}{j(\nu-1)}\right) + p_\nu.$$

The P-values on the RHS are the usual random field theory P-values for an F-statistic SPM with  $(j, \nu - j)$  df. The weights are

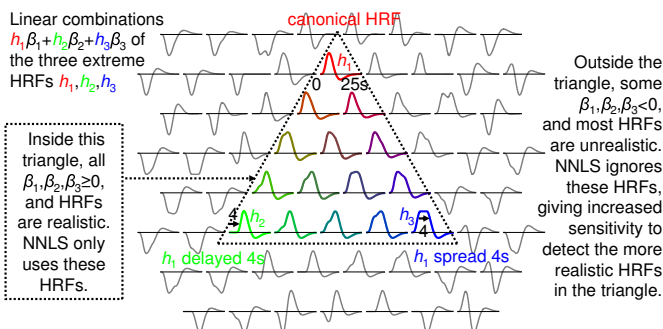
$$p_j = \mathbb{P}(\#\{\beta'_s > 0\} = j)$$

under  $H_0$ . In practice  $p_j$  is found by one simulation of Gaussian white noise under  $H_0$ , then averaging across voxels.

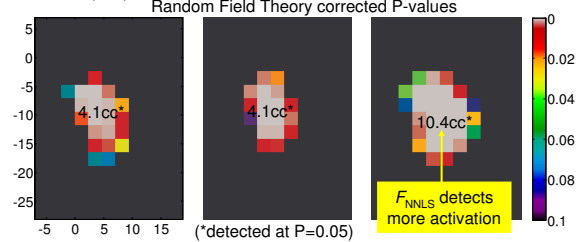
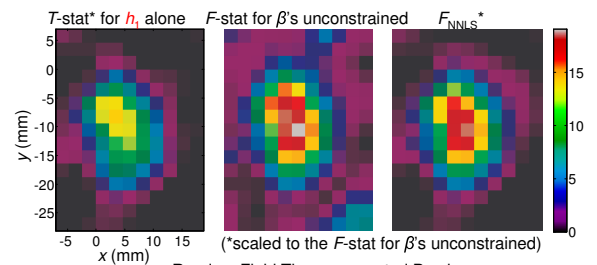
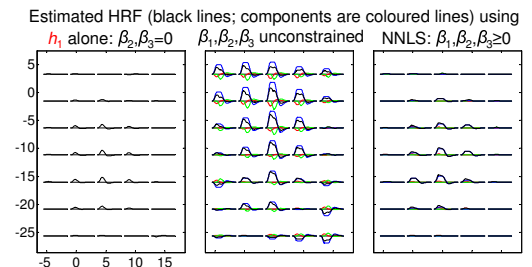
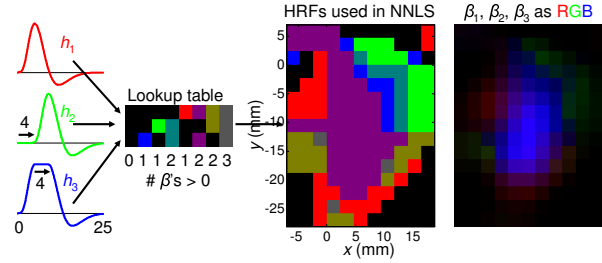
Surprisingly, it is possible to have far more regressors in  $\mathbf{X}$  than observations! If these regressors are highly correlated then  $\beta \geq 0$  forces  $p_j \sim 0$  for large  $j$ . An example is the spectral method for fitting compartmental models to PET data.

## Results

We apply these results to detecting activation in fMRI using a set of three extreme HRF basis functions:



A subject received a 9s painful heat stimulus alternating with a 9s warm stimulus interspersed with 9s rest, repeated 10 times [3]. The three columns of  $\mathbf{X}$  are the hot-warm stimuli convolved with the three extreme HRFs. The columns of  $\mathbf{Z}$  are the hot+warm stimuli convolved with the three extreme HRFs and spline drift regressors. The null degrees of freedom is  $\nu = 109$ . The weights were:  $p_1 = 0.498$ ,  $p_2 = 0.141$ ,  $p_3 = 0.003$ . Results in a small part of a slice through the right supplementary motor area are shown in the following figures.



## Conclusions

NNLS is more sensitive than either the T-statistic on the canonical HRF, or the F-statistic for the unconstrained model. The reason is that the T-statistic is not flexible enough to detect departures from the canonical HRF, whereas the unconstrained F-statistic is too flexible and wastes sensitivity on unrealistic (negative coefficient) HRFs.

## References

- [1] Lawson & Hanson (1974). *Solving Least Squares Problems*.
- [2] Taylor & Worsley (2007). Detecting sparse cone alternatives for Gaussian random fields... *Annals of Statistics*, submitted.
- [3] Worsley et al. (2002). *NeuroImage* 15:1-15.